

1 "Transcutaneous Medical Device Dressings and Method of Use"

2
3 **FIELD OF THE INVENTION**

4 The invention relates to transcutaneous medical device dressings, and processes for
5 their production and use, for controlling infections.

6 **BACKGROUND OF THE INVENTION**

7 *Sum (B1)*
8 Transcutaneous medical devices are catheters, pins, implants and the like which pass
9 through the skin and are indwelling for some considerable time. Exemplary of
10 transcutaneous medical devices are central venous catheters, peripheral venous catheters,
11 Swan-Gauz pulmonary catheters, central nervous system implants (ex. external ventricular
12 drainage and ventricular reservoirs), peritoneal dialysis catheters, such as for continuous
13 ambulatory peritoneal dialysis and continuous cyclic peritoneal dialysis, hemodialysis
14 catheters, transvenous pacemaker leads and temporary orthopedic pins. All of these
15 transcutaneous medical devices, when in place, have a portion of the device which is external,
16 that is which is left protruding from the skin, and which can be the the cause of infection.

17 The risk of acquiring infections from transcutaneous infections is very high. For
18 instance, the risk of acquiring catheter-related bloodstream infection ranges from 0.9 to 8%.
19 This nosocomial bloodstream infections cause a case fatality of more than 20%, and account
20 for an increase of thousands of dollars in hospital costs per infection, or tens of thousands of
21 dollars per survivor in ICU needing an extra week of hospital stay. As for peritoneal dialysis,
22 a very experienced center today still has a peritonitis rate of one episode per 15 to 25 patient
23 months. The major sources of bacteria in these infections are from surrounding skin.

24 To prevent infections associated with transcutaneous medical devices antiseptic
25 preparation of insertion sites, including the initial application of topical anti-microbial
26 solutions such as alcohol or iodine to the insertion sites is known. A further topical ointment
27 after insertion of the device, such as an ointment containing neomycin, polymyxin and
28 bacitracin, has been shown to prevent catheter colonization/infection, but it may increase the
29 risk of fungal infection. Ointments are also inconvenient, requiring multiple replacements.
30 There have also been attempts to attach a cuff to the catheters, with an anti-microbial agent
31 impregnated in the cuff. Efforts to coat the catheters with anti-microbial agents are known.
32 However, none of these efforts has been completely successful in clinical trials. Presently,
the most common catheter dressing used in hospitals comprises sterile gauze or polyurethane

1 film, which have limited infection control properties.

2 Recent efforts to replace gauze with a transparent film dressing to allow a visual
3 check on the insertion site is known, see for instance US Patent No. 5,372,589, issued
4 December 13, 1994 to Davis. No anti-microbial control is taught with such a dressing.
5 Johnson & Johnson Medical Inc. markets a product under the trade mark BIOPATCH, which
6 is a chlorhexidine gluconate-impregnated catheter patch. An Iodophor transparent dressing
7 has also been suggested. However, to date, no completely effective anti-microbial device for
8 use with transcutaneous medical devices is known.

9 A securement devices is taught for securing a intravenous device to the body in US
10 Patent 3,918,446, issued November 11, 1975 to Buttaravoli. The device has an upper and a
11 lower pad, between which the intravenous device is fixed. Since the function of the device is
12 to secure the device to the body, there is a teaching to provide an adhesive material to the
13 bottom of lower pad, and to the bottom of the top pad. There is a mention of providing the
14 adhesive with an antibacterial agent. This device has the disadvantage of using adhesives
15 with the antibacterial agent, which limits the effectiveness and long lasting ability of the
16 antibacterial agent. Furthermore, the adhesive can be irritating next to the skin, cause skin
17 damage and patient discomfort on removal, and inhibits the removal or changing of the
18 device. Furthermore, many adhesives act as moisture barriers, which can limit the
19 effectiveness of the antibacterial agent. Finally, the device of this patent teaches including a
20 slit in the bottom pad of the dressing, which lies below the intravenous needle or catheter
21 when the device is in place, allowing the intravenous device to remain in contact with the
22 skin, and therefore limiting the infection control of the device.

23 SUMMARY OF THE INVENTION

24 In one broad aspect, the invention provides a transcutaneous device dressing for use
25 with a transcutaneous medical device which has punctured the skin of a patient and which has
26 a portion of the medical device protruding from the skin, comprising:

27 a top and a bottom dressing, both being formed from a flexible material and having
28 upper and lower surfaces, with the lower surface being skin facing in use;

29 the bottom dressing having a slit formed therein extending from one edge inwardly to
30 a termination point within the confines of the bottom dressing;

31 an anti-microbial material provided without adhesives at the upper and lower surfaces
32 of the bottom dressing, and at least at the lower surface of the top dressing;

1 whereby, in use, the bottom dressing is placed next to the skin, the slit allowing the
2 bottom dressing to surround the puncture site such that the lower surface of the bottom
3 dressing is in contact with the skin and the upper surface of the bottom dressing is in contact
4 with a portion of the medical device protruding from the skin, and the top dressing is placed
5 above the puncture site such that its lower surface is in contact with a portion of the medical
6 device protruding from the skin, thereby exposing a portion of the medical device protruding
7 from the skin from above and below to the anti-microbial activity of the anti-microbial
8 material.

9 In another broad aspect, the invention provides a method of dressing the puncture site
10 of a transcutaneous medical device to limit infection by microorganisms from the
11 surrounding skin and the portion of the medical device that protrudes from the skin of a
12 patient, comprising:

13 providing a transcutaneous device dressing, comprising:

14 a top and a bottom dressing, both being formed from a flexible material and having
15 upper and lower surfaces, the lower surfaces being skin facing when the dressing is in use;
16 the bottom dressing having a slit formed therein extending from one edge inwardly to
17 a termination point within the confines of the bottom dressing; and

18 an anti-microbial material provided without the use of adhesives at the upper and
19 lower surfaces of the bottom dressing, and at least at the lower surface of the top dressing;

20 sliding the bottom dressing in place next to the skin using the slit to allow the bottom
21 dressing to surround the puncture site at the termination point such that the lower surface of
22 the bottom dressing is in contact with the skin surrounding the puncture site while the upper
23 surface of the bottom dressing is in contact with a portion of the medical device protruding
24 from the skin;

25 applying the top dressing above bottom dressing such that its lower surface is in
26 contact with a portion of the medical device protruding from the skin;

27 depending on the anti-microbial material, applying a water or alcohol based
28 electrolyte to the top and bottom dressings to release the anti-microbial agent; and

29 fixing the top and bottom dressings to the skin, preferably with an occlusive or semi-
30 occlusive layer such as an adhesive film.

31 The transcutaneous device dressing of this invention has the advantage of ease of
32 placement and been demonstrated to be much more effective than disc type dressings which

1 are laid flat under the transcutaneous device, which have only a limited portion, generally
2 only the thickness of the dressing (less than 3 mm), in contact with the portion of the medical
3 device which protrudes from the skin.

4 Preferably, the dressing of this invention is formed such that the top and bottom
5 dressings are joined along a fold line, that is they are formed from a unitary dressing which is
6 folded over in use. The slit is preferably formed from the edge of the bottom dressing which
7 is parallel to the fold. The dressing is preferably formed from multilayered, laminated
8 dressing materials. The anti-microbial material is preferably a thin film of an anti-microbial
9 metal, most preferably formed with atomic disorder so as to create an effective anti-microbial
10 effect, and to create an interference colour so as to provide an indicator, as described in
11 WO98/41095, published September 24, 1998, and naming inventors R. E. Burrell and R. J.
12 Precht.

13 The dressing of this invention has application to transcutaneous medical devices such
14 as listed above, made from a wide variety of materials, for example metals, including steel,
15 aluminum and its alloys, latex, nylon, silicone, polyester, polyurethane, and other plastics and
16 rubbers. Such devices are generally made of a bioinert or Biocompatible material. The
17 device may take a variety of shapes including rod or tube shapes, hollow or solid, and may be
18 rigid or flexible, factors dictated by its intended utility.

19 As used herein and in the claims, the terms and phrases set out below have the
20 meanings which follow.

21 "Metal" or "metals" includes one or more metals whether in the form of substantially
22 pure metals, alloys or compounds such as oxides, nitrides, borides, sulphides, halides or
23 hydrides.

24 "Anti-microbial metals" are metals whose ions have an anti-microbial effect.
25 Preferably, the metal will also be biocompatible. Preferred anti-microbial metals include Ag,
26 Au, Pt, Pd, Ir (i.e. the noble metals), Sn, Cu, Sb, Bi and Zn, with Ag being most preferred.

27 "Biocompatible" means non-toxic for the intended utility. Thus, for human utility,
28 biocompatible means non-toxic to humans or human tissues.

29 "Anti-microbial effect" means that atoms, ions, molecules or clusters of the anti-
30 microbial metal (hereinafter "species" of the anti-microbial metal) are released into the
31 alcohol or electrolyte which the material contacts in concentrations sufficient to inhibit
32 bacterial (or other microbial) growth in the vicinity of the material. The most common

1 method of measuring anti-microbial effect is by measuring the zone of inhibition (ZOI)
2 created when the material is placed on a bacterial lawn. A relatively small or no ZOI (ex. less
3 than 1 mm) indicates a non useful anti-microbial effect, while a larger ZOI (ex. greater than 5
4 mm) indicates a highly useful anti-microbial effect. One procedure for a ZOI test is set out in
5 the Examples which follow.

6 "Sustained release" or "sustainable basis" are used to define release of atoms,
7 molecules, ions or clusters of an anti-microbial metal that continues over time measured in
8 hours or days, and thus distinguishes release of such metal species from the bulk metal, which
9 release such species at a rate and concentration which is too low to achieve an anti-microbial
10 effect, and from highly soluble salts of anti-microbial metals such as silver nitrate, which
11 releases silver ions virtually instantly, but not continuously, in contact with an alcohol or
12 electrolyte.

13 "Atomic disorder" includes high concentrations of: point defects in a crystal lattice,
14 vacancies, line defects such as dislocations, interstitial atoms, amorphous regions, grain and
15 sub grain boundaries and the like relative to its normal ordered crystalline state. Atomic
16 disorder leads to irregularities in surface topography and inhomogeneities in the structure on
17 a nanometer scale.

18 "Normal ordered crystalline state" means the crystallinity normally found in bulk
19 metal materials, alloys or compounds formed as cast, wrought or plated metal products. Such
20 materials contain only low concentrations of such atomic defects as vacancies, grain
21 boundaries and dislocations.

22 "Diffusion", when used to describe conditions which limit diffusion in processes to
23 create and retain atomic disorder, i.e. which freeze-in atomic disorder, means diffusion of
24 atoms and/or molecules on the surface or in the matrix of the material being formed.

25 "Alcohol or water-based electrolyte" is meant to include any alcohol or water-based
26 electrolyte that the anti-microbial materials of the present invention might contact in order to
27 activate (i.e. cause the release of species of the anti-microbial metal) into same. The term is
28 meant to include alcohols, water, gels, fluids, solvents, and tissues containing water,
29 including body fluids (for example blood, urine or saliva), and body tissue (for example skin,
30 muscle or bone).

31 "Colour change" is meant to include changes of intensity of light under
32 monochromatic light as well as changes of hue from white light containing more than one

1 wavelength.

2 An "interference colour" is produced when light impinges on two or more partly
3 reflective surfaces separated by a distance which bears the right relationship to the
4 wavelength of the light to be removed by destructive interference.

5 "Partly reflective" when used to describe the base or top layer materials, means that
6 the material has a surface which reflects a portion of incident light, but which also transmits a
7 portion of the incident light. Reflection occurs when a ray of incoming light encounters a
8 boundary or interface characterized by a change in refractive index between two media. For
9 the top layer of the anti-microbial materials of this invention, that interface is with air. For
10 the base layer, the interface is with the top layer. The reflectance of the base and top layers is
11 balanced so as to generate an interference colour.

12 "Partly light transmissive" when used to describe a thin film of the top layer material
13 means that the thin film is capable of transmitting at least a portion of incident visible light
14 through the thin film.

15 "Detectable" when used to describe a colour change means an observable shift in the
16 dominant wavelength of the reflected light, whether the change is detected by instrument,
17 such as a spectrophotometer, or by the human eye. The dominant wavelength is the
18 wavelength responsible for the colour being observed.

19 DESCRIPTION OF THE DRAWINGS

20 Figure 1 is a schematic sectional figure of a three layer transcutaneous device dressing
21 in accordance with the present invention;

22 Figure 2 is a schematic perspective view of a three layer transcutaneous device
23 dressing folded along a central line to form top and bottom dressings and showing the slit for
24 placement around the transcutaneous medical device;

25 Figure 3 is a schematic sectional view of the folded transcutaneous device dressing in
26 place with a catheter penetrating the skin of a patient;

27 Figure 4 is a plan view of the transcutaneous device dressing of this invention,
28 showing the slit in the bottom dressing;

29 Figure 5 is a plan view of the transcutaneous device dressing slid in place with a
30 catheter, such that the bottom dressing is in contact with a portion of the catheter protruding
31 from the skin; and

32 Figure 6 is a plan view of transcutaneous device dressing folded such that the top

1 dressing is in contact with a portion of the catheter protruding from the skin.

2 **DESCRIPTION OF THE PREFERRED EMBODIMENTS**

3 Transcutaneous Device Dressing

4 The dressing in accordance with the invention includes at least one, and preferably at
5 least two or three layers of medical dressing materials, laminated together by known means
6 such as low temperature thermal fusing, stitching or, most preferably, ultrasonic welding. A
7 three layer dressing in accordance with the invention is shown generally at 10 in Figure 1 to
8 include a first layer 12, which will be skin facing in use, a second layer 14, which preferably
9 forms an absorbent core, and a third layer 16. The layers 12, 14 and 16 are shown to be
10 laminated together by ultrasonic welds 18 at intermittent locations across the dressing 10.

11 Figure 2 shows the dressing 10 to comprise a top dressing 20 and a bottom dressing
12 22 formed from the three layers 12, 14 and 16. In Figure 2, the top and bottom dressings 20,
13 22 are joined along a fold line 24, being formed from a unitary dressing 10. However, in
14 accordance with this invention, the top and bottom dressings 20, 22 may be formed from
15 separately, from same or different medical dressing materials. If the top and bottom dressings
16 20, 22 are provided separately, the top dressing 20 may include an occlusive or semi-
17 occlusive layer such as an adhesive film (not shown) in order to secure the dressing 10 in
18 place, and retain moisture for activation of the anti-microbial material. A slit 26 is formed in
19 the bottom dressing 22, preferably extending from the edge of the bottom dressing 22 which
20 is parallel to the fold line 24, and terminating at a termination point 28 which is preferably
21 about the center point of the bottom dressing 22.

22 The dressing 10 is shown in place against the skin 30 of a patient in Figure 3, with a
23 catheter 32 protruding from the skin 30 at a penetration site 34. The dressing is held in place
24 against the skin with an occlusive or semi-occlusive layer 36, such as adhesive tape or
25 polyurethane film. The dressing is sized to cover a significant portion of the catheter 32 that
26 protrudes from the skin 30, and not just the immediate skin area surrounding the penetration
27 site. This aids in limiting infection, since bacteria are prevented from migrating along the
28 catheter 32. A minimum dressing size will preferably provide at least 5 mm coverage of the
29 protruding catheter 32, more preferably 1 - 5 cm coverage.

30 Depending on the size of the transcutaneous medical device, the termination point 28
31 of the slit 26, may include additional cuts, preferably a cross-cut, or a penetrating hole (not
32 shown), to allow the medical device to fit through the dressing, while still maintaining the

1 portions around the termination point in close contact with both the skin and protruding
2 section of the medical device.

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5 Figures 4, 5 and 6 demonstrate placement of the dressing 10 around a catheter 32,
6 with the bottom dressing 22 sliding under the catheter 32 such that the lower surface 36 (see
7 Figure 2) of the bottom dressing 22 contacts the patient's skin (not shown), while the upper
8 surface 38 of the bottom dressing 22 contacts the catheter 32 protruding from the skin. Once
9 the top dressing 20 is applied, by folding it over the bottom dressing 22, the lower surface 40
10 (see Figure 2) of the top dressing 20 is in contact with the catheter 32 protruding from the
11 skin. The upper surface 42 of the top dressing 20 is then covered with the occlusive or semi-
12 occlusive layer 36, as shown in Figure 3. As shown in Figures 4 and 5, when the dressing 10
13 is formed from a unitary dressing, the lower surface 40 of the top dressing 20 and the upper
14 surface 40 of the bottom dressing 22, are one and the same layer, represented as layer 16 in
15 Figure 1.

16 The lower and upper surfaces 38 and 40 of the bottom dressing 22, and at least the
17 lower surface 42 of the top dressing 20 are provided with an anti-microbial material in order
18 to limit infection. Anti-microbial materials for use with medical dressing materials are well
19 known in the art. The anti-microbial material may be impregnated in one or more of the
20 layers of the dressing 10, but will more preferably be provided as a thin film of an anti-
21 microbial metal on those surfaces of the top and bottom dressings 20, 22 which will be skin
22 or catheter facing once the dressing is in place. Alternatively, the anti-microbial material may
23 be an antibiotic composition or a composition formed from an anti-microbial metal, as are
24 well known in the art.

25 The preferred and alternate compositions of the layers 12, 14 and 16, together with the
26 preferred anti-microbial metal coatings are set out in further detail below.

27 Dressing Materials

28 The first layer 12 of the dressing 10 is formed of a perforated, preferably non-adherent
29 material which allows for fluids to penetrate or diffuse there through in either or both
30 directions. The perforated material may be formed of a woven or non-woven, non-woven
31 being preferred, fabric such as cotton, gauze, a polymeric net or mesh such as polyethylene,
32 nylon, polypropylene or polyester, an elastomer such as polyurethane or polybutadiene
elastomers, or a foam such as open cell polyurethane foam. Exemplary perforated, non-
adherent materials useful for the dressing include non-woven meshes such as DELNET™

1 P530, which is a non-woven veil formed of high density polyethylene using extrusion,
2 embossing and orientation processes, produced by Applied Extrusion Technologies, Inc. Of
3 Middletown, Delaware, USA. This same product is available as Exu-Dry CONFORMANT
4 2TM Wound Veil, from Frass Survival Systems, Inc., Bronx, New York, USA as a subset of
5 that company's Wound Dressing Roll (Non-Adherent) products. Other useful non-woven
6 meshes include CARELLETM or NYLON 90TM, available from Carolina Formed Fabrics
7 Corp., N-TERFACETM, available from Winfield Laboratories, Inc., of Richardson, Texas,
8 USA. Exemplary woven meshes may be formed from fibreglass or acetate, or cotton gauze.
9 An exemplary hydrophilic polyurethane foam is HYPOLTM, available from W.R. Grace &
10 Co., New York, NY, USA.

11 For ease of ultrasonic welding for lamination, at least one of the first and second
12 layers 12, 14 is preferably formed from a polymeric material which is amenable to ultrasonic
13 welding, that is which will melt on the application of localized heat and then fuse the layers
14 together on cooling.

15 The second, absorbent layer 14 is formed from an absorbent material for holding
16 sufficient moisture next to the skin in order to activate the anti-microbial metal coating, that
17 is to cause release of ions, molecules, atoms or clusters of the anti-microbial metal in order to
18 cause an anti-microbial effect. Preferably, the absorbent material is an absorbent needle
19 punched non-woven rayon/polyester core such as SONTARATM 8411, a 70/30
20 rayon/polyester blend commercially available from Dupont Canada, Mississauga, Ontario,
21 Canada. This product is sold by National Patent Medical as an American White Cross sterile
22 gauze pad. However, other suitable absorbent materials include woven or non-woven
23 materials, non-woven being preferred made from fibers such as rayon, polyester,
24 rayon/polyester, polyester/cotton, cotton and cellulosic fibers. Exemplary are creped
25 cellulose wadding, an air felt of air laid pulp fibers, cotton, gauze, and other well known
26 absorbent materials suitable for medical dressings.

27 The third layer 16 of the dressing 10 is preferably formed of perforated, non-adherent
28 material such as used in the first layer 12. This allows moisture penetration as sterile water
29 and the like are added in order to activate the anti-microbial metal coating.

30 Additional layers (not shown) may be included between or above the first, second and
31 third layers 12, 24, 16, as is well known in medical. Thus the use of the terms first, second
32 and third layer, as used herein and in the claims is not meant to exclude such additional

1 layers.

2 The layers 12, 14, and 16 laminated together at intermittent spaced locations across
3 the dressing 10 by ultrasonic welds 18. Ultrasonic welding is a known technique in the
4 quilting art, and thus will not be discussed at length. Briefly, heat (generated ultrasonically)
5 and pressure are applied to either side of the dressing 10 at localized spots through an
6 ultrasonic horn so as to cause melting of at least one of the plastic materials in the first and
7 second layers 12, 14, and the subsequent bonding together of the layers on cooling. The
8 welds appear at localized circular spots and are preferably less than 0.5 cm in diameter. If the
9 third layer 16 is present, the ultrasonic welding can be performed from either side of the
10 dressing, and will bind all three layers 12, 14 and 16 together.

11 The use of ultrasonic welding of the layers at spaced locations has the advantage of
12 retaining the absorbent and moisture penetration properties of the layers 12, 14, while
13 retaining the conforming properties of the dressing. Edge seams, stitching and adhesives
14 have the disadvantage of interfering with one or more of these desirable properties of the
15 dressings. Furthermore, by spacing the welds 18 at intermittent locations across the dressing,
16 the dressing 10 may be cut to smaller sizes, as needed, without causing delamination.
17 Preferred spacings of about 2.5 cm between welds allows the dressing to be cut down to
18 about 2.5 cm sizes, while maintaining at least one weld to hold the laminated layers together.

19 Anti-Microbial Coating

20 The dressing 10 of this invention preferably includes an anti-microbial coating formed
21 from an anti-microbial metal. The coating is applied to one or more of the layers 12, 14, 16,
22 but is most preferably applied at least to the first and third layers 12 and 16, so as to provide
23 the anti-microbial effect both against the skin and against the transcutaneous medical device
24 held between the top and bottom dressings 20, 22.

25 The coating is most preferably formed with atomic disorder in accordance with the
26 procedures set out above and as described in US Patent 5,454,886, and WO98/41095, both to
27 Burrell et al. Most preferably, the coating is formed as a multilayer anti-microbial coating
28 having a top and a base layer, as set below, to produce an interference colour. In this way, the
29 coating provides not only an anti-microbial effect to limit infection, but also acts as an
30 indicator of activation of the dressing. As the top layer of the coating is activated with an
31 alcohol or water-based electrolyte, such as sterile water or ethanol, even minor dissolution of
32 the anti-microbial metal results in a detectable colour change, indicating that an anti-

1 microbial effect is being provided. If there is no colour change, additional moisture might be
2 provided to the dressing by adding water, until a colour change is detected. Once activated,
3 the dressing should be maintained in a moist condition by the addition of sterile water if
4 necessary.

5 Sterilization

6 Dressings 10 with anti-microbial coatings of an anti-microbial metal formed with
7 atomic disorder are preferably sterilized without applying excessive thermal energy, which
8 can anneal out the atomic disorder, thereby reducing or eliminating a useful anti-microbial
9 effect. Gamma radiation is preferred for sterilizing such dressings, as discussed in US Patent
10 5,454,886.

11 It should be appreciated that the use of ultrasonic welding to laminate the layers of
12 dressings with anti-microbial coatings formed from anti-microbial metals with atomic
13 disorder is advantageous since it achieves bonding in localized spots and avoids applying heat
14 to any significant portion of the dressing, thereby avoiding any significant reduction in the
15 anti-microbial effect through annealing out of atomic disorder.

16 The sterilized dressings should be sealed in packaging which excludes light
17 penetration to avoid additional oxidation of the anti-microbial coating. Polyester peelable
18 pouches are preferred. The shelf life of anti-microbial dressings thus sealed is over one year.

19 Directions for Use of Dressings with Transcutaneous Devices

20 With transcutaneous devices such as flexible catheters, the dressing 10 is placed on
21 the skin around the catheter 32 by passing the catheter 32 through the slit 26. The dressing 10
22 is rotated, if needed, to ensure that slit 26 is roughly perpendicular to the long axis of the
23 catheter 32, thus ensuring that the portion of the catheter 32 protruding from the skin is
24 contacted by the upper surface 40 of the bottom dressing 22. The top dressing 20 is folded
25 over the bottom dressing 22 (or placed over, if the top and bottom dressings are separate),
26 such that the lower surface 42 of the top dressing 20 is in contact with the portion of the
27 catheter 32 protruding from the skin. If the anti-microbial material is an anti-microbial metal
28 coating, the dressing is then moistened with drops of sterile water or 70% ethanol, in order to
29 activate the coating for release of anti-microbial metal species. The dressing 10 is then
30 secured in place with an occlusive or semi-occlusive layer 36, such as an adhesive film,
31 which keeps the dressing in a moist environment.

32 If the transcutaneous device is rigid, such as a temporary orthopedic pin, the bottom

1 dressing 22 is put in place as set out above, but the top dressing 20 is then folded and secured
2 around the portion of the pin protruding from the skin, in a tent-like manner, since the pin
3 generally protrudes at an angle normal to the skin surface.

4 Animal trials with the dressing of the present invention, carrying a bi-layer anti-
5 microbial coating formed with silver having atomic disorder, manufactured as set out above
6 and as described in greater detail in Example 3, have shown excellent results in controlling
7 infection. In use, the dressings are kept moist, at 100% relative humidity. Adding sterile
8 water initially to activate the anti-microbial metal coating is needed, and then as needed to
9 maintain the dressing in a moist condition. Dressings may be changed as required for
10 observation and cleaning, but need not be changed more frequently than every 7 days, and
11 can provide an anti-microbial effect for a much longer period of time.

12 Multilayer Anti-Microbial Materials With Interference Colour

13 The dressings preferably include the anti-microbial metal coating formed with at least
14 two metal layers, a base layer and a top layer over the base layer, so as to produce an
15 interference colour, as set forth in WO98/41095. Both layers are partly reflective; the top
16 layer is partly light transmissive. The top layer is a thin film containing at least one anti-
17 microbial metal formed with sufficient atomic disorder such that the top layer, in contact with
18 an alcohol or water based electrolyte, releases ions, atoms, molecules or clusters of the anti-
19 microbial metal at a concentration sufficient to provide a localized anti-microbial effect on a
20 sustainable basis. In this way, the top layer, in contact with the alcohol or electrolyte, will
21 undergo a change in optical path length, either by a change in thickness resulting from some
22 dissolution, or through a change in the refractive index of the top layer resulting from a
23 change in the composition of a newly formed thin layer formed on the top layer. Either or
24 both of these results are sufficient to cause a detectable colour change, thus providing an
25 indicator that the top layer has been activated.

26 Both the base layer and the top layer are formed from a partly reflective material. In
27 this way, at least a portion of the incoming light is reflected from the surface of the layer
28 while another portion is transmitted through the layer. The top layer is partly light
29 transmissive to allow incident light to reach the interface with the base layer. The top layer
30 thus cannot approximate 100% reflectivity, such as in pure Al or Ag, or interference colours
31 cannot be generated, as is well known in the art. The materials for the top and base layers
32 should be balanced in their reflectances in order to generate an interference colour.

1 Generally, the top layer is deposited as a thin film having a thickness which maintains
2 adequate transmittance to generate an interference colour. Furthermore, the refractive index
3 for the materials in layers is different, accomplished by differences in their actual or effective
4 compositions. For instance different materials in the two layers will result in the materials
5 having different actual refractive indexes. However, if it is desired to make the layers from
6 the same material, the layers can be deposited with different porosities or different
7 levels/types of atomic disorder, in order to achieve different effective compositions, and thus
8 different refractive indexes.

9 In this manner, incoming light reflects off the interface of the base and top layers.
10 Incoming light reflects from the interface of the top layer with air, and interferes with the
11 light reflected from the interface with the base layer so as to generate an "interference
12 colour". The particular colour which is generated and its brightness will depend on the
13 properties of the layers, most importantly on the composition of the layers, which determines
14 its transmittance and absorption properties, along with its refractive index, and on the
15 thickness of the layers. Generally, it is desirable to generate first and second order
16 interference colours, by limiting the thickness of the base layer and top layers to minimize the
17 number of internal reflections. First and second order interference colours are generally
18 brighter than third and fourth order etc. colours, making them more aesthetically pleasing,
19 more consistently reproducible in manufacturing, and more susceptible to detectable colour
20 change on variations in thickness on dissolution of even a minor amount of the top layer.

21 The property which determines the particular colour which is generated is the
22 effective optical thickness of the top layer, that is the product of the refractive index of the
23 top layer material and the actual thickness of the top layer. Thus the colour which is desired
24 can be altered by changing the actual thickness or the top layer or its refractive index.

25 Preferably, the material in the base layer is a reflective metal. Such metals are known
26 in the art and include, for example one or more of the valve metals, e.g., Ta, Nb, Ti, Zr and
27 Hf, as well as transition metals such as Au, Ag, Pt, Pd, Sn, Cu, V, W and Mo, or the metal Al.
28 More preferably, the base material is formed from Ag, Au, Pt, Pd, Cu, Ta and Al. Use of a
29 metal such as tantalum as the base layer may cause reduction of oxide containing materials in
30 the top layer. To avoid this, a barrier layer (not shown), such as tantalum oxide formed by
31 anodizing at least a portion of the top surface of the Ta metal, should be included above a
32 tantalum layer. Preferred metals for the base layer are the anti-microbial metals Au, Ag, Pt,

1 Pd, Sn and Cu, more preferably Au, Pt and Ag, and most preferably Ag, in a partly reflective
2 form.

3 The base layer may be formed by known techniques, such as the vapour deposition
4 techniques of evaporation or physical vapour deposition. Preferably, the base layer is formed
5 as a thin film by physical vapour deposition with atomic disorder, as set out below and in US
6 5,454,889, in order to produce a sustainable anti-microbial effect when the base layer is
7 ultimately exposed to an alcohol or water based electrolyte. The thickness of the base layer is
8 generally not critical, provided that it is partly reflective. Preferred thicknesses will vary
9 widely with the material composition and the desired colour. However, in that the layer is
10 preferably a thin film formed by physical vapour deposition techniques, it should be at least
11 about 25 nm thick to create a useful colour. To generate first and second order interference
12 colours and to produce an anti-microbial effect, the base layer should be greater than 60 nm
13 thick, more preferably 300 to 2500 nm thick, and most preferably 600 to 900 nm thick.

14 The top layer is formed of a partly reflective, partly light transmissive thin film
15 containing at least one anti-microbial metal formed with atomic disorder so as to produce a
16 sustainable anti-microbial effect, and ultimate colour change, when exposed to an alcohol or a
17 water based electrolyte. The anti-microbial metal is preferably one or more of Ag, Au, Pt,
18 Pd, Ir, Sn, Cu, Sb, Bi, and Zn in a partly reflective, partly transmissive form. More
19 preferably, the anti-microbial metal is Ag, Au, Pt, Pd or Cu. The thickness of the top layer
20 formed from these metals is preferably less than 400 nm in order to maintain the preferred
21 level of light transmission. The desired thickness will vary with the composition of the top
22 layer, and with the desired end colour and colour change. For first and second order
23 interference colours, the thickness will generally be less than about 400 nm. More preferably,
24 the thickness will range from 5 to 210 nm, most preferably from 10 to 100 nm.

25 The top layer may be a thin film of the base layer material, formed with a different
26 refractive index for instance by altering the deposition conditions to change the porosity,
27 composition and/or degree of atomic disorder in the layers.

28 When the base layer is itself formed from an anti-microbial metal with atomic
29 disorder, the top layer may be provided as an in situ generated top layer by virtue of its
30 thickness and/or composition changing on contacting an alcohol or water based electrolyte, so
31 as to produce an interference colour which differs from the initial colour of the base layer.

32 Most preferably, the top layer is a thin film of a composite material formed by co-,

1 sequentially or reactively depositing an anti-microbial metal in a matrix with atoms or
2 molecules of a different material to create atomic disorder in the matrix, in the manner set out
3 below. The different material is selected from a) biocompatible metals, b) oxygen, nitrogen,
4 hydrogen, boron, sulphur or halogens, or c) an oxide, nitride, carbide, boride, halide, sulphide
5 or hydride of either or both of an anti-microbial metal or a biocompatible metal. Most
6 preferably, the top layer material is a composite material containing silver, and one or both of
7 silver oxide and atoms or molecules containing oxygen trapped or absorbed in the silver
8 matrix. The term "silver oxide" is meant to include any oxide or mixture of oxides of silver.
9 However, the top layer is preferably not formed solely of AgO and/or Ag₂O, since the
10 solubility of these materials is low for providing a useful anti-microbial effect.

11 Anti-Microbial Materials Containing Atomic Disorder

12 At least the top layer, and preferably also the base layer, is formed in a crystalline
13 form from anti-microbial metals with atomic disorder so as to produce an anti-microbial
14 effect. The production of atomic disorder through physical vapour deposition techniques is
15 described in U.S. 5,454,886, and as outlined below.

16 The anti-microbial metal is deposited as a thin metallic film on one or more surfaces
17 of the dressing 10, by vapour deposition techniques. Physical vapour techniques, which are
18 well known in the art, all deposit the metal from the vapour, generally atom by atom, onto a
19 substrate surface. The techniques include vacuum or arc evaporation, sputtering, magnetron
20 sputtering and ion plating. The deposition is conducted in a manner to create atomic disorder
21 in the coating as defined above. Various conditions responsible for producing atomic
22 disorder are useful. These conditions are generally those which one has been taught to avoid
23 in thin film deposition techniques, since the object of most thin film depositions is to create a
24 defect free, smooth and dense film (see for example J.A. Thornton, supra). While such
25 conditions have been investigated in the art, they had not been linked to enhanced solubility
26 of the coatings so-produced prior to Applicants inventions.

27 The preferred conditions which are used to create atomic disorder during the
28 deposition process include:

29 - a low substrate temperature, that is maintaining the surface to be coated at a
30 temperature such that the ratio of the substrate temperature to the melting point of the metal
31 (in degrees Kelvin) is less than about 0.5, more preferably less than about 0.35 and most
32 preferably less than about 0.3; and optionally one or both of:

1 - a higher than normal working (or ambient) gas pressure, i.e. for vacuum
2 evaporation: e-beam or arc evaporation, greater than 0.01 mT, gas scattering evaporation
3 (pressure plating) or reactive arc evaporation, greater than 20 mT; for sputtering: greater than
4 75 mT; for magnetron sputtering: greater than about 10 mT; and for ion plating: greater than
5 about 200 mT; and

6 - maintaining the angle of incidence of the coating flux on the surface to be
7 coated at less than about 75°, and preferably less than about 30°

8 The metals used in the coating are those known to release ions etc. having an anti-
9 microbial effect, as set out above. For most dressings, the metal must also be biocompatible.
10 Preferred metals include the noble metals Ag, Au, Pt, Pd, and Ir as well as Sn, Cu, Sb, Bi, and
11 Zn or alloys or compounds of these metals or other metals. Most preferred is Ag or Au, or
12 alloys or compounds of one or more of these metals.

13 For economic reasons, the thin metal film has a thickness no greater than that needed
14 to provide release of metal ions on a sustainable basis over a suitable period of time, and to
15 generate the desired interference colour. Within the preferred ranges of thicknesses set out
16 above, the thickness will vary with the particular metal in the coating (which varies the
17 solubility and abrasion resistance), and with the degree of atomic disorder in (and thus the
18 solubility of) the coating. The thickness will be thin enough that the coating does not
19 interfere with the dimensional tolerances or flexibility of the device for its intended utility.

20 The anti-microbial effect of the material so produced is achieved when the coating is
21 brought into contact with an alcohol or a water based electrolyte, thus releasing metal ions,
22 atoms, molecules or clusters. The concentration of the metal species which is needed to
23 produce an anti-microbial effect will vary from metal to metal. Generally, anti-microbial
24 effect is achieved in body fluids such as plasma, serum or urine at concentrations less than
25 about 0.5 - 5 µg/ml.

26 The ability to achieve release of metal atoms, ions, molecules or clusters on a
27 sustainable basis from a coating is dictated by a number of factors, including coating
28 characteristics such as composition, structure, solubility and thickness, and the nature of the
29 environment in which the device is used. As the level of atomic disorder is increased, the
30 amount of metal species released per unit time increases. For instance, a silver metal film
31 deposited by magnetron sputtering at $T/T_m < 0.5$ and a working gas pressure of about 7
32 mTorr releases approximately 1/3 of the silver ions that a film deposited under similar

1 conditions, but at 30 mTorr, will release over 10 days. Films that are created with an
2 intermediate structure (ex. lower pressure, lower angle of incidence etc.) have Ag release
3 values intermediate to these values as determined by bioassays. This then provides a method
4 for producing controlled release metallic coatings. Slow release coatings are prepared such
5 that the degree of disorder is low while fast release coatings are prepared such that the degree
6 of disorder is high.

7 For continuous, uniform coatings, the time required for total dissolution will be a
8 function of film thickness and the nature of the environment to which they are exposed. The
9 relationship in respect of thickness is approximately linear, i.e. a two fold increase in film
10 thickness will result in about a two fold increase in longevity.

11 It is also possible to control the metal release from a coating by forming a thin film
12 coating with a modulated structure. For instance, a coating deposited by magnetron
13 sputtering such that the working gas pressure was low (ex. 15 mTorr) for 50% of the
14 deposition time and high (ex. 30 mTorr) for the remaining time, has a rapid initial release of
15 metal ions, followed by a longer period of slow release. This type of coating is extremely
16 effective on devices such as urinary catheters for which an initial rapid release is required to
17 achieve immediate anti-microbial concentrations followed by a lower release rate to sustain
18 the concentration of metal ions over a period of weeks.

19 The substrate temperature used during vapour deposition should not be so low that
20 annealing or recrystallization of the coating takes place as the coating warms to ambient
21 temperatures or the temperatures at which it is to be used (ex. body temperature). This
22 allowable ΔT , that the temperature differential between the substrate temperature during
23 deposition and the ultimate temperature of use, will vary from metal to metal. For the most
24 preferred metals of Ag and Au, preferred substrate temperatures of -20 to 200°C , more
25 preferably -10°C to 100°C are used.

26 Atomic order may also be achieved, in either or both of the base and top layers by
27 preparing composite metal materials, that is materials which contain one or more anti-
28 microbial metals in a metal matrix which includes atoms or molecules different from the anti-
29 microbial metals.

30 The preferred technique for preparing a composite material is to co- or sequentially
31 deposit the anti-microbial metal(s) with one or more other inert, biocompatible metals
32 selected from Ta, Ti, Nb, Zn, V, Hf, Mo, Si, Al and alloys of these metals or other metal

1 elements, typically other transition metals. Such inert metals have a different atomic radii
2 from that of the anti-microbial metals, which results in atomic disorder during deposition.
3 Alloys of this kind can also serve to reduce atomic diffusion and thus stabilize the disordered
4 structure. Thin film deposition equipment with multiple targets for the placement of each of
5 the anti-microbial and inert metals is preferably utilized. When layers are sequentially
6 deposited the layer(s) of the inert metal(s) should be discontinuous, for example as islands
7 within the anti-microbial metal matrix. The final ratio of the anti-microbial metal(s) to inert
8 metal(s) should be greater than about 0.2. The most preferable inert metals are Ti, Ta, Zn and
9 Nb. It is also possible to form the anti-microbial coating from oxides, carbides, nitrides,
10 sulphides, borides, halides or hydrides of one or more of the anti-microbial metals and/or one
11 or more of the inert metals to achieve the desired atomic disorder.

12 Another composite material may be formed by reactively co- or sequentially
13 depositing, by physical vapour techniques, a reacted material into the thin film of the anti-
14 microbial metal(s). The reacted material is an oxide, nitride, carbide, boride, sulphide,
15 hydride or halide of the anti-microbial and/or inert metal, formed in situ by injecting the
16 appropriate reactants, or gases containing same, (ex. air, oxygen, water, nitrogen, hydrogen,
17 boron, sulphur, halogens) into the deposition chamber. Atoms or molecules of these gases
18 may also become absorbed or trapped in the metal film to create atomic disorder. The
19 reactant may be continuously supplied during deposition for codeposition or it may be pulsed
20 to provide for sequential deposition. The final ratio of anti-microbial metal(s) to reaction
21 product should be greater than about 0.2. Air, oxygen, nitrogen and hydrogen are particularly
22 preferred reactants.

23 The above deposition techniques to prepare composite coatings may be used with or
24 without the conditions of lower substrate temperatures, high working gas pressures and low
25 angles of incidence previously discussed. One or more of these conditions are preferred to
26 retain and enhance the amount of atomic disorder created in the coating.

27 Examples

28 Example 1

29 This example shows the preparation of a bilayer anti-microbial silver coating on a
30 dressing material. A high density polyethylene dressing, DELNET™ or CONFORMANT
31 2™ was coated with a silver base layer and a silver/oxide top layer to generate a coloured
32 anti-microbial coating having indicator value. The coating layers were formed by magnetron

1 sputtering under the conditions set out in Table 1.

2 Table 1

10201

3 <u>Sputtering Conditions:</u>	<u>Base Layer</u>	<u>Top Layer</u>
4 Target	99.99% Ag	99.99% Ag
5 Target Size	20.3 cm diameter	20.3 cm diameter
6 Working Gas	96/4 wt% Ar/O ₂	96/4 wt% Ar/O ₂
7 Working Gas Pressure	40 mTorr	40 mTorr
8 Power	0.3 kW	0.15 kW
9 Substrate Temperature	20°C	20°C
10 Base Pressure	3.0 X 10 ⁻⁶ Torr	3.0 X 10 ⁻⁶ Torr
11 Anode/Cathode Distance	100mm	100mm
12 Sputtering Time	7.5 - 9 min	1.5 min
13 Voltage	369 - 373 V	346 V

14 The resulting coating was blue in appearance. A fingertip touch was sufficient to
15 cause a colour change to yellow. The base layer was about 900 nm thick, while the top layer
16 was 100 nm thick.

17 A zone of inhibition test was conducted. Mueller Hinton agar was dispensed into
18 Petri dishes. The agar plates were allowed to surface dry prior to being inoculated with a
19 lawn of *Staphylococcus aureus* ATCC#25923. The inoculant was prepared from Bactrol
20 Discs (Difco, M.) Which were reconstituted as per the manufacturer's directions.
21 Immediately after inoculation, the coated materials to be tested were placed on the surface of
22 the agar. The dishes were incubated for 24 hr. at 37°C. After this incubation period, the
23 zone of inhibition was calculated (corrected zone of inhibition = zone of inhibition - diameter
24 of the test material in contact with the agar). The results showed a corrected ZOI of about 10
25 mm.

26 The coating was analyzed by nitric acid digestion and atomic absorption analysis to
27 contain 0.24 +/- 0.04 mg silver per mg high density polyethylene. The coating is a binary
28 alloy of silver (>97%) and oxygen with negligible contaminants, based on secondary ion
29 mass spectroscopy. The coating, as viewed by SEM, was highly porous and consisted of
30 equiaxed nanocrystals organized into coarse columnar structures with an average grain size of
31 10 nm. Silver release studies demonstrated that silver was released continuously from the
32 coating until an equilibrium concentration of about 66 mg/L was reached (determined by
33 atomic absorption), a level that is 50 to 100 times higher than is expected from bulk silver
34 metal (solubility \leq 1mg/L).

35 By varying the coating conditions for the top layer to lengthen the sputtering time to 2

1 min, 15 sec., a yellow coating was produced. The top layer had a thickness of about 140 nm
2 and went through a colour change to purple with a fingertip touch. Similarly, a purple
3 coating was produced by shortening the sputtering time to 1 min, to achieve a top layer
4 thickness of about 65 nm. A fingertip touch caused a colour change to yellow.

5 Example 2

6 This example is included to demonstrate a multilayer transcutaneous device dressing
7 in accordance with the present invention. High density polyethylene mesh dressing material
8 DELNET™ or CONFORMANT 2™ dressing was coated with a bilayer blue anti-microbial
9 coating as set forth in Example 1, using the sputtering conditions of Table 1. Two layers of
10 this coated dressing material were placed above and below an absorbent core material formed
11 from needle punched rayon/polyester (SONTARA™ 8411). With the silver coating on both
12 the first and third layers, the dressing may be used with either the blue coating side or the
13 silver side in the skin facing position. For indicator value, it might be preferable to have the
14 blue coating visible. The three layers were laminated together by ultrasonic welding to
15 produce welds between all three layers spaced at about 2.5 cm intervals across the dressing.
16 This allowed the dressing to be cut down to about 2.5 cm size portions for smaller dressing
17 needs while still providing at least one weld in the dressing portion.

18 The coated dressings were sterilized using gamma radiation and a sterilization dose of
19 25 kGy. The finished dressing was packaged in sealed individually polyester peelable
20 pouches, and has shown a shelf life greater than 1 year in this form. The coated dressings can
21 be cut in ready to use sizes, such as 5.1 x 10.2 cm strips, and slits formed therein before
22 packaging. Alternatively, the dressings may be packaged with instructions for the clinician to
23 cut the dressing to size and form the desired length of the slit for the medical device.

24 Example 3

25 This animal study evaluated four prototype catheter dressings, one of which was in
26 made in accordance with Example 2 above, the others being 3 cm disc shaped catheter
27 dressings of laminated dressing materials, having a thickness less than about 1 mm, formed
28 with a slit to their center to fit beneath the catheter, and being coated with a silver coating
29 deposited as in Example 1. The silver coatings were prepared in a full scale roll coater under
30 conditions to provide coatings having the same properties set out in Examples 2 and 3 above.

31 The prototype dressings were as follows:

- 32 1. Silver Catheter Dressing, prepared as in Example 2, with a top and a bottom

1 dressing sized 5.1 x 5.1 cm, with a 2.6 cm slit in the bottom dressing, as an
2 example of this invention.

- 3 2. Silver Disc 1 - A 3 cm disc of the dressing material of Example 2, but used
4 only as a flat disc beneath the catheter (i.e., with no top dressing)
- 5 3. Silver Disc 2 - A 3 cm disc of the dressing material which included a first
6 layer of silver coated DELNET, as set out in Example 1, laminated to
7 STATEX, AET, 8.0NP₂-A/QW, which is a layer of 100% rayon on a
8 polyurethane film, used as a flat disc beneath the catheter (i.e. with no top
9 dressing)
- 10 4. Silver Foam Disc 3 - A 3 cm disc formed of three layers of silver coated high
11 density polyethylene prepared as in Example 1, alternating with two layers of
12 polyurethane foam, L-00562-6 Medical Foam, available from Rynel Ltd.,
13 Bootbay, Maine, USA, used as a flat disc beneath the catheter (i.e., with no top
14 dressing).

15 Fifteen healthy New Zealand white rabbits weighing 2.6 to 2.9 kg were used.
16 Segments of polyurethane catheters (Arrow polyurethane indwelling central venous catheters,
17 16 Ga, from Arrow International, Inc., Reading, PA, USA, cut to 5 cm long) were implanted
18 subcutaneously in the back of the rabbits. The rabbits were anesthetized with halothane
19 (University of Calgary, LESARC SOP A6 - Life & Environmental Sciences Animal Resource
20 Centre, Standard Operating Procedures). The dorsal thorax and abdomen were clipped and
21 scrubbed with non-antibiotic soap. A scalpel was used to make a cut on the skin. A 5 cm
22 long catheter segment was then inserted into subcutaneous tissue space perpendicular to the
23 spine. Six catheters were implanted in each rabbit. The catheter sites were dressed with each
24 of the prototype catheter dressings or control gauzes, such that the protruding portion of the
25 catheter passed through the slit of the disc or dressing. In the case of the dressing of this
26 invention, Silver Catheter Dressing, the top layer was placed over the catheter and pressed
27 down so that the dressing surrounded the segment of the catheter protruding from the skin.
28 The catheters were sutured to the skin. Three rabbits were dressed with each type of dressing
29 or control dressing.

30 Bacterial challenges of each site were made by placing bacterial suspension-soaked
31 gauzes (10 x 12.5 cm) on the tops of the dressings. In this inoculation technique the gauzes
32 used were larger than the test dressings and were in contact with the heads of the catheters

which protruded above the dressings, as a result the gauzes provided sources of bacteria to the surrounding skin, the catheter dressings and the catheter heads. Five milliliters of bacterial suspension (*Staphylococcus aureus* ATCC 25923, grown in TSB (tryptic soy broth) overnight, washed with PBS (phosphate buffered saline) and re-suspended in PBS, concentration adjusted to 10^7 CFU/ml (colony forming unit)) was inoculated at each catheter site. An occlusive tape was then placed over the dressing to ensure a moist environment inside.

The rabbits were observed for seven days and then euthanized on Day 7. The skin was dissected and the inside portion of catheter was carefully exposed. Catheter sections (1 cm) were cut from the proximal and distal sites to the skin entrance and collected in tubes containing 2 ml of STS (0.4% sodium thioglycolate, 0.85% sodium chloride and 1% TweenTM 20). Adherent bacteria were recovered from the proximal and distal sites of the catheters by sonication and vortexing. The solutions were plated on TSA plates using a drop-plate method and bacterial counts were recorded.

During the whole test period, all dressings or discs remained in place, although some curling and folding occurred on three of the Disc 1 type discs. The results of the colonization rates and bacteria counts for the proximal and distal sites of the implanted catheters are presented in Table 2, with means of n (shown in parentheses) samples. The numbers in parenthesis following the colonization rates represent numbers of colonized/total catheters.

Table 2 Catheter Colonization Rates and Bacterial Recovery from Catheters

Dressing Type	Colonization Rate (%)	Bacterial Counts for the Proximal Site (CFU/cm)	Bacterial Counts for the Distal Site (CFU/cm)
Silver Catheter Dressing	0 (0/18)	0	0
Silver Disc 1	38.8 (7/18)	1.8×10^3 (n=7)	5.8×10^2 (n=9)*
Silver Disc 2	47.1 (8/17)	4.6×10^3 (n=8)	3.2×10^2 (n=6)
Silver Foam Disc 3	33.3 (6/18)	1.4×10^3 (n=6)	3.0×10^2 (n=2)
Control	94.4 (17/18)	7.6×10^4 (n=17)	4.1×10^3 (n=11)

* Two distal sites had 50 CFU/cm (only one colony was found in one of the duplicate plates, while the proximal sites of the same catheters had no bacteria). This may have been because of contamination. These two sites were not included when the colonization rate was

1 calculated for this group.

2 The data showed that with gauze coverage, 94.4 % of the catheters were contaminated
3 with bacterial counts averaging over 10^4 CFU/cm. With regard to the Silver Catheter
4 Dressing of this invention, it completely prevented bacterial colonization. The disc type
5 dressings, Discs 1, 2 and 3 reduced catheter contamination rates to 38.8%, 47% and 33.3 %,
6 respectively. It is expected that these disc dressing materials would reduce catheter
7 contamination to a sufficiently low rate if a top dressing of the same material was used with
8 the discs, in accordance with the present invention.

9 All publications mentioned in this specification are indicative of the level of skill of
10 those skilled in the art to which this invention pertains. All publications are herein
11 incorporated by reference to the same extent as if each individual publication was specifically
12 and individually indicated to be incorporated by reference.

13 The terms and expressions in this specification are, unless otherwise specifically
14 defined herein, used as terms of description and not of limitation. There is no intention, in
15 using such terms and expressions, of excluding equivalents of the features illustrated and
16 described, it being recognized that the scope of the invention is defined and limited only by
17 the claims which follow.